The Treatment of Intertrochanteric Fractures of the Femur with Proximal Femoral Nail

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SUMMARY

Background. The incidence of fractures in the trochanteric area has risen with the increasing numbers of elderly persons with osteoporosis. The imperative goals of treatment are early mobilization by means of stable fixation using as minimally invasive a procedure as possible. Nowadays, there is an increasing interest in intramedullary nailing, especially for unstable intertrochanteric fractures. The aim of the present paper is to assess the efficacy of closed intramedullary osteosynthesis with the proximal femoral nail (Endovis®) in the treatment of peritrochanteric fractures to solve the problems associated with the use of intramedullary fixation devices.

Material and methods. The authors describe their experience with 87 stable and unstable proximal extracapsular femoral fractures treated with the Endovis femoral nail from July 2007 to March 2009. The results were evaluated clinically, functionally and radiographically during the 1st, 3rd, 6th and 12th months post-op. Pre-injury activity and functional levels were recorded using the modified Harris hip score and V.A.S. score.

Results. Postoperative radiographs showed a near-anatomical fracture reduction in 85% of patients. Three were the cases of cut-out, one case of valgus and two cases of shortening of the operated leg (<1 cm). The Harris Hip Score increased between the thirtieth and ninetieth postoperative day, accompanied by a significant decrease in pain symptoms and functional limitation.

Conclusions. 1. The application of an intramedullary nail provides primary stability of the fracture. 2. The Endovis nail constitutes a powerful synthesis for stable and unstable fractures of the trochanteric region, in which is difficult to reconstruct appropriate continuity between the medial and posterior cortical layers. 3. The good mechanical stability of the nail allows rapid mobilization and early functional recovery. 4. The presence of an additional anti-rotational screw and the free sliding mechanism of the lag screw may increase rotational stability of cervico-cephalic fragments and decrease overload on the femoral head.

Key words: hip fracture, endomedullary nail, inter-trochanteric fracture, fracture fixation, bone nails.
BACKGROUND

Intertrochanteric fractures constitute one of the commonest fractures of the hip. The incidence of fractures in the trochanteric area has risen with the increasing numbers of elderly persons with osteoporosis [1,2]. Although a large number of different implants are available for fixation, the ideal implant for the treatment of intertrochanteric fractures is still a matter for discussion. The imperative goals of treatment are early mobilization by means of stable fixation using as minimally invasive a procedure as possible. Nowadays, there is an increasing interest in intramedullary nailing, especially for unstable intertrochanteric fractures [3,4,5]. Several clinical and biomechanical studies have analysed the results of different implants such as the dynamic hip screw (DHS), the Gamma nail (GN) and the proximal femoral nail (PFN). Those devices have suffered cut-out, implant breakage, femoral shaft fractures and subsequent loss of reduction in the clinical setting [6,7,8]. However, preoperative and postoperative technical complications are common in some cases, necessitating a new surgical treatment. The Endovis® proximal femoral nail (EN) has been designed by Citieffe® (Italy) to solve the problems associated with the use of intramedullary fixation devices. Some studies have demonstrated a good outcome with few complications after treatment with this intramedullary femoral nail [9,10]. EN is made of a titanium alloy with a cervicodiaphyseal angle of 130 degrees, a metaphyseal angle of 5 degrees and a total length of 195 mm (standard nail) or 220 mm (medium nail). The diameter is 13 mm (standard nail) or 13.5 mm (medium nail) proximally and 10 mm distally. There are two holes for cephalic screw insertion and one for the distal screw. The cephalic screws are available in nine length sizes, 7.5 mm diameter, self-drilling and self-taping. The distal screw is available in four sizes, 5 mm diameter, self-drilling and self-taping. The distal tip of the nail has a diapason section (Tab. 1).

MATERIALS AND METHODS

EN was performed in 87 patients with proximal extra-capsular femoral fractures at the Department of Orthopaedic Surgery of the University of Palermo between July 2007 and March 2009 (Tab. 2). There were 69 (79.3%) females and 18 (20.7%) males in the group, with a mean age of 72.3 years (range: 56-91). In accordance with the recommendations of the AO/ASIF (Fig. 1), the preoperative radiographs were classified as 31-A1 (stable pertrochanteric) in 33 patients, 31-A2 (unstable pertrochanteric) in 37, and 31-A3 (unstable intertrochanteric) in 17 (Fig. 2). During surgery, all fractures were treated by closed reduction under C-arm fluoroscopy guidance. Spinal anaesthesia was used in all patients. All operations were performed by the same group of experienced surgeons. The intramedullary femoral nail used was the EN in its standard or medium design (Fig. 3). The surgical technique followed the manufacturer’s instructions. The intramedullary nail was interlocked proximally with two screws (cephalic and anti-rotational) and distally with one or 2 screws. The operative time, blood loss during surgery, fluoroscopy time, and the amount of blood transfused were recorded. After a closed reduction of the fracture, a long-

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<th>Tab. 1. Characteristics of standard and medium Endovis nail</th>
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<td><strong>Material</strong></td>
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<td>Cervicodiaphyseal angle</td>
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<th>Tab. 2. Epidemiology of the study group</th>
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<td><strong>ENDOVIS NAIL (N=87)</strong></td>
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<td>Male</td>
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<td>Age</td>
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<td>Type of fracture: 31 A 1</td>
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itudinal incision started proximal to the greater trochanter apex and extended proximally about 4-10 cm, depending on the size or obesity of the patient. After splitting the aponeurosis, the entry point was made just on the tip of the greater trochanter. The nail was inserted into the femoral diaphysis without reaming. Our goal was to insert the hip screw under the midline of the femoral neck, advancing the tip of the screw close to the subarticular surface of the femoral head. Tip to Apex Distance (TAD) was measured from the tip of the guide wire. When TAD was less than 25 mm, we proceeded to reaming and insertion of the cephalic screw. Fluoroscopic screening was performed to ensure that the joint line was not penetrated after screw placement. Distal locking was made preferably with 2 screws. In all cases antithrombotic prophylaxis was given using low molecular weight heparin (Fraxiparine), and antibiotic prophylaxis was provided (Cefazolin). The rehabilitation protocol was identical, and the patients were mobilised on the first postoperative day. Patients were allowed to mobilise on postoperative day 2, and weight-bearing walking was initiated on day 3 or 4 as tolerated. The average follow-up period was 12 months (range 9-18 months). Clinical and radiographic examinations were performed at the time of admission and at three, six and 12 months postoperatively. We noted any change in the position of the implants and the progress of fracture union. A minimum follow-up of 3 months was required. The average follow-up period was 6.5 months (range, 4 to 21 months). Pre-injury activity and functional levels were recorded using the modified Harris hip score and VAS score.

RESULTS
The mean time needed for the two intramedullary Endovis nails procedures was 24.4 minutes (range, 18-47). In 90% of the patients, the fracture was the result of a domestic fall; in the remaining 10%, it had been caused by a vehicular accident. Perioperative fluoroscopy screening lasted a mean of 137 seconds (104-159 seconds). In AP radiographs, 100% of the lag screws appeared to be placed in the inferior part of the femoral head. In lateral radiographs, 90% of the lag screws appeared to be placed centrally, 8% anteriorly, and 2% posteriorly. Mean blood loss was 120 ml (80-200). Three patients required blood transfusion with a mean volume of 1.5 units. Mean hospital stay was 7 days (5–11 days). Postoperative radiographs showed a near-anatomical fracture reduction in 85% of the patients (Fig. 4). According to the Garden alignment index, 71 cases were classified as very good, nine cases as good and seven as satisfactory. Implant positioning with an average TAD of 18.9 mm (range 9–30 mm) was acceptable. The patients were followed up at 3, 6 and 12 months. There were no cases of deep infection and no failures or breakages due to implant fatigue. Fracture of the greater trochanter during insertion of the nail was seen in one patient, who was treated conservatively. Six patients (6.8%) died in the first year and two patients (2.3%) were lost to follow up after 6 months. Repeat surgery was necessary in five patients (5.7%). Four cases of cut-out (Fig. 5) were noted. They were associated with malposition of the proximal lag screws and were treated using a new intramedullary Endovis nail. One patient had a traumatic fracture of the femoral shaft below the tip of the implant. This case was treated using an Endovis long nail (340 mm). Moreover, one case of valgus was revealed. Three patients demonstrated medial displacement of the femoral diaphysis with consequent shortening of the affected femur. All fractures were considered clinically healed within three months in all patients, with the exception of those with mechanical failure, who needed reoperation. Active and passive exercises

Fig. 1. AO Classification System of Proximal lateral femoral fractures
Fig. 2. Type and distribution of proximal extra-capsular femoral fracture in the study

Fig. 3. Standard and medium Endovis nail

Fig. 4. Pertrochanteric fracture type 31A2 treated with Endovis medium nail
were initiated within 48 h of surgical treatment. The
VAS scale on the second day had an average of
9 (range 7-10), compared to 7 (range 5-9) on day 30,
6 (range 5-7) on day 90, and 4 (range 1-6) on day 90.
The Harris Hip Score increased between the thirtieth
and ninetieth postoperative day from an average of
60 to 85, accompanied by a significant decrease in
pain symptoms and functional limitation (Fig. 6).

DISCUSSION
Trochanteric fractures occur mostly in elderly pa-
tients, and the outcome may be extremely poor if
there is prolonged bedrest.

An osteoporosis-related decrease [11] in the me-
chanical properties of bone leads to frequent fractu-
res following low-energy injuries, usually a fall at
ground level. Peritrochanteric fractures of the femur
occur much less frequently in younger persons and
are mostly due to high-energy injuries such as traffic
accidents or falls from a height.

Surgery is the mainstay of treatment for both dis-
placed and non-displaced intertrochanteric fractures. The
primary reason for surgery is to allow early mo-
bilization of the patient, with partial weight-bearing
restrictions depending on the stability of the reduction
[12]. The ideal implant for stabilization of pertro-
chanteric fractures is still under debate. Many inter-
nal fixation devices have been recommended for the
treatment of pertrochanteric fractures, including extra-
medullary and intramedullary implants [13,14]. The
dynamic hip screw (DHS), initially introduced by
Clawson in 1964, remains the implant of choice be-
cause of its favourable results and low rate of non-
union and failure [15,16]. This implant consists of
a large lag screw placed in the centre of the femoral
neck and head and a side plate along the lateral femur
The screw-plate interface angle is variable and depends on the anatomy of the patient and the fracture. The advantage of the sliding lag screw, compared with the static screw, is that it allows for impaction of the fragments; this impaction increases the bone-on-bone contact, promoting osseous healing while decreasing implant stress; the disadvantage is shortening and rotation at the fracture site, both of which are commonly encountered [18]. Although repair of an intertrochanteric fracture is often referred to as open reduction with internal fixation (ORIF), the term closed reduction with internal fixation (CRIF) may be more accurate. However, intramedullary nails have been gaining popularity for both stable and unstable fractures, due to certain theoretical advantages and technical ease; additionally, the small incisions result in less intraoperative blood loss. A variety of intramedullary devices have been used with different design characteristics. The main principle of this type of fixation is based on a sliding screw in the femoral neck-head fragment, attached to an intramedullary nail. The GN has been available since 1988 and was designed specifically for the treatment of these fractures in order to combine the advantages of semiclosed intramedullary nailing, a dynamic femoral nail screw and early post-operative weight-bearing. High incidence (6-17%) of femoral shaft fractures after Gamma nailing was observed in earlier studies (19, 20). It was believed that this was due to design specifics of the first generation Standard Gamma Nail, such as the length, the valgus curvature and the distal diameter. It has also been suggested that there is a disparity between the design of the nail and the geometry of the bone resulting in increased stiffness of the bone-implant system [21]. Inappropriate placement of the distal locking screws and/or misdrilling could also be responsible for some of these complications. The PFNA system was developed by the AO/ASIF in 2004. The main design characteristic of the implant is the use of a single blade with a large surface area. Insertion of the blade compact the cancellous bone. Biomechanical tests have demonstrated that the blade has a significantly higher cut-out resistance than commonly used screw systems [22].

However, the adequacy and stability of fixation plays an important role, determining the success of surgical treatment of pertrochanteric fractures [23]. The EN is fixed with 2 screws; the larger (lag) screw is designed to carry most of the load, and the smaller screw (the hip pin) is to provide rotational stability. If the hip pin is longer than the lag screw, vertical forces would increase on the hip pin and start to induce cut-out, a knife effect or Z-effect. The right position of the lag screw near the centre of the femoral head and neck, in both anteroposterior and lateral views, is critical and has been emphasized by many authors. Baumgartner et al. [24] indicated the significance of tip-apex distance value in the placement of the proximal lag screw and Den Hartog [25] showed that this optimal position prevents the rotation of the femoral head and neck during lag screw insertion. The lag screw should be inserted into the femoral head as deeply as noted in the AP view, and centrally in the lateral view. The tip of the lag screw should always be inferior to the centre of the femoral head. Anatomic and biomechanical studies have shown that the superomedial quadrant of the femoral head is the weakest part for the implant, and therefore proper positioning of the screw is emphasised. Cut-out is usually the result of poor positioning of the proximal screw in the femoral head, particularly in osteoporotic bone. The cut-out rate with a PFN-A is reportedly 0.6 to 8% [26, 27]. The complication of cut out was often reported in the literature when trochanteric fractures were treated with gamma nail [28,29]. Makridis et al. [30] studied cut-out in 64 patients. Three cases of cut-out, associated with malposition of the proximal lag screws, occurred with the ENDOVIS nail. In a study of Véronail, another nail, Lavini et al. [31] observed screw cut-out in 4.5% of cases. In our study, the lag screw was inserted close to the subchondral bone, and the hip pin superior to the femoral head. We used two lag screws in our EN design in order to enhance stability and to decrease the incidence of lag screw cut-outs. In our study cut-out was observed in 4 patients (4.7%). Anatomical fracture reduction and the insertion of the inferior lag screw as close as possible to the inferior cortex of the femoral neck is strongly recommended because the compression trabeculae and tensile trabeculae of the proximal femur intersect at the inferior part of the femoral neck, constituting the strongest architecture. However, our study revealed that the Endovis blade cut-out can be due to inadequate insertion. Careful and adequate insertion of the blade or lag screw may be a more important consideration than biomechanical stability. In this study, operating time and operative blood loss seemed to be identical compared with a previous study of the other intramedullary femoral nail. The Endovis femoral nail was developed to solve such problems as the perioperative and postoperative technical complications described in patients treated with the gamma nail. According to the literature, these complications, which necessitate reoperation, occur in 3% to 7% of cases. The ambulatory status after an operation for an intertrochanteric fracture depends on a number of factors. Specific parameters
such as the patients’ preoperative walking capability, their medical condition and comorbidities were similar in both groups. The overall walking competence in patients treated with the Endovis was very high. An improvement to 44% of the pre-operative modified Harris score was achieved during the hospitalisation period; this increased to 83% after 4 months. This compares very favourably with other published studies; in the largest single series of patients treated with the DHS this was 35.1%.

CONCLUSIONS

1. The application of an intramedullary nail (EN) provides primary stability of the fracture, whose synthesis is then completed from the cervico-cephalic screws and possibly from the distal locking screws.

2. The EN constitutes a powerful synthesis for stable and unstable fractures of the trochanteric region in which it is difficult to reconstruct appropriate continuity between the medial and posterior cortical layers.

3. The good mechanical stability of the nail allows rapid mobilization and early functional recovery and provides a self-sufficient solution for older persons who need a quick and good recovery for physical and psychological reasons.

4. The presence of an additional anti-rotational screw and the free sliding mechanism of the lag screw may increase rotational stability of cervico-cephalic fragments and decrease overload on the femoral head.

REFERENCES